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IMMUNODIAGNOSTIC DEVICE

BACKGROUND OF THE INVENTION

The device and methodology described herein facilitates diagnostic assays involving the formation and detection of particulate complexes, particularly immune complexes, which are difficult or impractical to perform. Traditional methods of testing for particulate complexes are time-consuming and costly, primarily due to the repetitive steps required to carry out the assay, as well as the complexity of the laboratory equipment needed to accomplish it. Further, such tests often necessitate intermediate extraction and washing steps to eliminate interfering substances present in the sample.

A key goal in developing immunodiagnostic test systems is to reduce the time it takes for the user to complete the assay. Consequently, considerable effort has been expended towards reducing the number of steps required to carry out the assay, with the ultimate goal of having a single step assay. The latter presently does not exist.

In addition to decreasing the time it takes to perform the diagnostic test, another desirable property of such systems is that they be stable at room temperature for prolonged periods of time. Generally, diagnostic devices comprise several reagents having different temperature stabilities. Some of these reagents are stable at room temperature for short periods of time, while others are even less stable, or not stable at all. The effect of temperature on the reagents decreases the sensitivity, and reliability of the assay, and increases the background. Most commercial diagnostic devices presently available

require that one or more of the reagents used to effect the assay be kept at low temperature to ensure its stability. Indeed, table 1 shows that either the entire diagnostic kits, or the reagents present in the kit, of the three major suppliers that produce hormone pregnancy kits, must be stored at low temperature to be effective. Thus, a diagnostic test system that is room temperature stable for long periods of time would have a clear advantage over state of the art devices.

Most diagnostic devices presently in use are premised on the "sandwich" assay. Here, the analyte, or substance sought to be assayed, is incubated with an excess of antibody molecules bound to solid matrix material. Subsequently, a labeled second antibody, also in excess, but directed against a second determinate on the analyte is incubated with the immune complex formed from the first antibody attached to the solid matrix material. The presence of labeled antibody on the surface of the immune complex is determined by suitable means depending on the type of label used. This type of assay is commonly referred to as a "sandwich", or "2-site" assay, since the antigen has two antibodies bound at two different regions, or epitopes.

A number of "sandwich" assays have been patented (see, for example, U.S. Patent 4,361,647, or 4,497,899). Despite their widespread use, their performance is not without difficulty. As alluded to above, they require successive manipulations, and suffer from low sensitivity. For instance, a generally used procedure for conducting an immunoassay using the "sandwich" technique involves:

1. Determining the working dilutions of the antibody;
2. Removing any excess antibody used to sensitize the solid matrix material;
3. Washing the solid support matrix free of unbound antibody;
4. Contacting the matrix with the test assay solution;
5. Incubating for extended periods of time the analyte to be detected in the test assay sample so as to allow the analyte to bind to the antibody;
- 10 6. Washing the matrix to remove any unreacted material;
7. Contacting the matrix with labeled second antibody;
8. Washing the solid matrix material to remove any unreacted second antibody;
- 15 9. Determining the presence of the immuno complex, either directly if the second antibody is radio labeled using suitable counting techniques, or if the label is an enzymatic label by adding a substrate that yields a detectable color change upon reaction.
- 20 10. In the instance where the second antibody carries an enzymatic label, after a period of time to allow sufficient color intensity to develop, the reaction is stopped with strong alkaline, or acid.
In addition to being time-consuming and relatively insensitive, "sandwich" assays are further limited in two other respects; first they are not readily adaptable for use with devices to detect more than one antigenic substance present in a sample. Thus, if one wishes to test a sample for multiple antigens, separate aliquots of the sample
30 must be assayed independently. Second, they often make

inefficient use of assay sample, thereby necessitating having to assay large sample volumes to obtain a reliable result.

In part this is because the sample is deposited over a
5 large surface area of solid matrix material. Thus, a device premised on the sandwich technique that facilitate assaying multiple antigens, and that makes more efficient use of sample fluid would be a clear advance over state of the art devices.

10 As alluded to above, an appealing feature presently lacking in diagnostic devices is long term room temperature stability. At present all the reasons for instability have not been identified. However, it appears that part of the cause is due to instability of antibody bound to the solid
15 support matrix, and the formation of aggregates in the antibody-enzyme conjugate employed to detect the presence of antigen. The former problem has not been satisfactorily dealt with while the formation of aggregates can be controlled by storing the conjugate at temperatures in the range of two to
20 eight degrees centigrade. At these temperatures the rate of aggregate formation is reduced. However, because it is inconvenient, and expensive to store the diagnostic device at low temperature, considerable effort has been expended to develop antibody-enzyme conjugates that are stable at room
25 temperatures, or methods to reduce the background arising from the aggregates. To date these efforts have been unsuccessful.

Another concern in performing diagnostic assays is to separate immunoreactants that do not bind antigen, and thus
30 do not form part of the immune complex, from bound reactants

that form the complex. The presence of unbound reactants can increase the background of the assay. While washing the immune complex can, and, indeed, does remove most of the background signal due to unbound reactants, most assays 5 employ what is termed a blocking step to further reduce the background. The blocking step involves coating the solid support with proteinaceous substances after it has been coated with antibody. The blocking material binds to sites on the solid matrix material which are not covered with 10 antibody, and thus prevents subsequent nonspecific binding of immune reactants that are not part of the immune complex. Generally, the blocking step is performed either before the assay is conducted, hence, necessitating an additional time consuming step, or else, as described in U.S. Patent 15 3,888,629, the solid matrix material is impregnated with the blocking agent, and then freeze dried and maintained in this state prior to use. The inconvenience in having to pretreat the solid surface with blocking material, or using freeze dried filters, with blocking proteins contained 20 therein, is tedious, time-consuming, and costly. Thus, a method that avoids both of these procedures would yield a more desirable diagnostic device.

In light of the above, it is apparent that while there exists many immunodiagnostic devices, it is desirable to 25 increase their sensitivity, ease and speed of performance as well as their long term room temperature stability.

SUMMARY OF INVENTION

An immunodiagnostic assay device is described that has considerable advantages over present state of the art 30 devices, and can be used to perform both sandwich and

nonsandwich assays. It has several features that in combination yield a device that is stable at room temperature for long times, yields results quickly, is highly sensitive, and, moreover, is capable of 5 simultaneously detecting more than one antigen present in the same assay solution.

It will be appreciated by those skilled in the art that while the diagnostic assay device described herein is anticipated to be primarily employed in assaying either 10 antigens or antibodies through the formation of an immune complex, that in fact, its applicability is considerably broader, and is not restricted to these molecules. At a minimum, the device merely requires a first molecule that recognizes and binds a second molecule. The first molecule 15 can be conveniently termed a ligand-recognition molecule, and the latter a ligand. While antibody and antigen are preferred embodiments of a ligand-recognition molecule and ligand respectively, the device can be used with a variety of ligands and ligand-recognition molecules. For example, 20 hormone receptor molecules are a type of ligand recognition molecule and can be attached to the solid matrix material, and used to assay for the corresponding hormone ligand. Alternatively, a hormone could be bound to the matrix material and used to assay for hormone receptors. It will be 25 apparent to those skilled in the art that there are many such combinations of ligand-recognition molecules and ligands suitably employable in the present immunodiagnostic device.

If either a sandwich or nonsandwich assay is employed 30 in the present device, a matrix material is impregnated with

antibody using a novel printer-coder technique comprising applying one or more distinct antibodies to the matrix by spraying them directly onto it. Using this technique, it is possible to rapidly deposit antibodies in discrete circles,
5 lines, or other geometric shapes for binding one or more antigens. Thus, the number of antigens that can be assayed is a function of the number of different antibodies that can be applied in distinct patterns.

Beneath the antibody impregnated matrix material are
10 two discrete layers of absorbent materials. Directly beneath the matrix material is a mid-layer of material that decreases the background. Further removed from the matrix material is the second layer of absorbent material. Its function is to absorb and hold assay or wash fluids, and can
15 be composed of a wide variety of absorbent materials.

Another aspect of the invention described herein that reduces background activity is a prefilter impregnated with suitable blocking material, particularly, but not exclusively, proteinaceous material. The prefilter is
20 situated over the matrix material, and is impregnated with blocking material by contacting the filter under defined conditions with proteinaceous material. When the assay is performed, a suitable amount of assay fluid is applied to the prefilter which passes through the prefilter carrying
25 the blocking material with it. The assay fluid, and the blocking materials contained therein contact the antibody impregnated matrix material wherein the blocking material binds to nonspecific reactive sites on the matrix material, thereby making these sites unavailable for binding by excess
30 immunochemicals involved in effecting the assay.

An additional feature of the subject invention that contributes to its sensitivity, and long term room temperature stability, is that it can be carried out in a chamber having at least two compartments. One compartment 5 contains the antibody impregnated matrix material, while the second compartment can contain moisture absorbent chemicals. The latter communicates with the former, and enhances the sensitivity and reliability of the assay since it maintains a desiccant like environment in the first compartment. This 10 favorably maintains the stability of the blocking agent in the prefilter, and the antibody associated with the matrix material during prolonged periods of nonuse. The same effect can be realized, albeit not as conveniently, by associating the moisture absorbent chemicals with the prefilter and 15 matrix material by other means.

A further feature associated with the present invention is a funnel shaped aperture in the roof of the device that provides access of assay fluid to the matrix material. This design makes efficient use of assay sample, and subsequent 20 washes, by depositing them over a small surface area of matrix material.

It will be understood by those skilled in the art that while the immunodiagnostic device has been described in terms of assaying for antigen by binding antibody to the 25 matrix material, that its usefulness is not so limited. It will be appreciated that it is suitably employed to assay for antibodies present in assay fluids by attaching their corresponding antigens to the matrix material. This aspect of the invention may aid the detection and diagnosis of 30 auto-immune diseases.

The combination of features associated with the diagnostic device described herein yields a system that is more sensitive than those presently in use, is reliable, convenient to use, has broad applicability, and, moreover, 5 can be stored at room temperatures for long periods of time without loss of activity.

BRIEF DESCRIPTION OF DRAWINGS

FIGURE 1 is a perspective view of the diagnostic unit; FIGURE 2 is an exploded view showing the various 10 components; and

FIGURE 3 is an enlarged sectional view taken on line 3-3 of FIGURE 1.

DETAILED DESCRIPTION OF THE INVENTION

It will be apparent to those skilled in the art that 15 the essence of the present invention is a filter impregnated with blocking agent, matrix material suitably impregnated with antibody, an absorbent layer for removing excess fluids, and a container for supporting and associating all the above to effect an immunoassay. Thus, while the 20 invention is described below in considerable detail, this description represents the preferred embodiment of the invention, and should not be construed as limiting the invention.

Figures 1 & 2 show a representative example of a 25 suitable immunodiagnostic test device useable in the present invention. Figure 1 shows a fully assembled, and Figure 2 an exploded view of the device. As shown in Figure 1, it comprises a container 10, having a separable top section 12, and a bottom section 14 and a filtering device 28. Figure 2 30 further reveals the container 10 and the top 12 and bottom

sections 14. In a preferred embodiment of the invention the bottom section 14 is separated into two chambers 16 and 18. Situated in chamber 16 is absorbent material 20 that receives fluid from the mid-layer 22. The mid-layer 22 in 5 turn receives fluid from matrix material 24. Also shown in Figure 2 are notches 40 that act as vents for pressure equilibration when the top 12 and bottom sections 14 are joined. The latter reduce the time it takes to perform the assay, but are not essential to carrying out the assay.

10 The top section 12 of the container 10 has an aperture 26 contained therein. When the top section 12 is aligned with the bottom section 14, by posts 13 affixed to the top section that fit into holes 15 in the bottom section, the aperture is positioned over the matrix material 24.

15 Further, the top section 12 has associated with it a filtering device 28. The filtering device 28 is situated over the aperture 26 such that when fluid is applied to the filtering device 28, the filtrate passes through the aperture 26 and contacts the matrix material 24. The 20 filtering device 28 is associated with the top section 12 by any one of a number of means. It is convenient to accomplish this by having post 30 at the corners of the device 28 fit into receptacles 32 situated on the top section 12.

25 Both the aperture 26 and the filtering device 28 preferably have a funnel shape configuration. This permits a large amount of sample fluid to be passed through a small amount of surface area of the matrix material 24. While the dimensions of both the aperture 26 and the filtering device 30 28 can be varied considerably without affecting the

performance of the device, we have found the following approximate dimensions to be satisfactory; 1.0 cm bottom diameter, 2.0 cm top diameter, and 0.3 cm deep.

A feature of the subject invention which allows for
5 long term storage without deterioration of the reagents present in the filtering device 28, or the matrix material 24, is a moisture absorbing chemical situated in the chamber 18. Such chemicals prevent moisture from contacting the reagents and causing a loss in activity. A variety of
10 chemicals well known to those skilled in the art are useful for this purpose. It should be apparent that the effectiveness of the present invention is not absolutely reliant on a device having a chamber 18 for holding moisture absorbing chemicals. A single chamber will perform
15 adequately provided the chemicals are otherwise associated with it, for example by disposing them on the outside.

Figure 3 shows an enlarged sectional view of the present invention. The filtering device 28 is affixed to the top section 12 by posts 30 that are situated in holes 32.
20 The top section 12 and bottom section 14 are also joined by posts 13 situated in the top section that fit into holes 15 in the bottom section.

It will be appreciated by those skilled in the art that while the container that forms the diagnostic device shown
25 in figures 1-3 has a flat configuration, that the invention is not limited to this shape. Virtually, any shape will perform adequately provided it has associated with it the elements described above.

The present diagnostic device is useful for detecting a
30 ligand-ligand recognition molecule complex on a solid

surface. It is important to note that either the ligand, or the ligand-recognition molecule can be bound to the matrix material 24, and be used to detect the corresponding member of the complex. That is, if the ligand-recognition molecule 5 is bound to the matrix material, then generally, the ligand can be assayed; however, if the ligand is bound to the matrix material 24, then the ligand-recognition molecule can be assayed.

Ligands are generally, but not necessarily, small 10 molecular weight molecules such as drugs, peptide hormones, and other bioactive molecules. Ligand-recognition molecules, on the other hand, are generally, but also not necessarily, large molecular weight molecules, being most often protein, particularly antibody molecules. Thus, it 15 will be understood by those skilled in the art, that while the subject diagnostic device preferred embodiment is antigen and antibody (mono or polyclonal), as ligand and ligand-recognition molecule respectively, the invention is not limited to the use of this pair of ligand and ligand- 20 recognition molecules. However, because these are most often used in diagnostic assay procedures, the invention will be described with reference to them.

The diagnostic device described herein will most often be used to detect a "sandwich" immune complex formed of 25 antibody and antigen, and thus will employ a support material as the matrix 24 suitable for binding a nonlabeled first antibody. It will be appreciated however, that the device is equally capable of being used to perform nonsandwich assays, particularly competitive binding assays. 30 The latter are often employed to assay small molecular

weight molecules that either have a single antibody binding site, or, because of their size, prevent more than one antibody from binding due to steric hindrance. Thus, the invention can be used to assay drugs, steroids, and the like.

Attachment of the antibody to the solid matrix material may be by absorption, or by covalent linkage, directly, or through a linker of sorts well-known to those skilled in the art. Suitable methods of carrying out these procedures, among a wide variety, are given for example by Iman and Hornby in Biochemical Journal (1972), Volume 129; Page 255; Campbell, Hornby, and Morris in Biochem. Biophys. Acta (1975), Volume 384; Page 307; and Mattisson and Nilsson in F.E.B.S. letters, (1977) Volume 104, Page 78. Moreover, chemically pretreated materials suitable for coupling antibodies can be purchased commercially.

Numerous materials can be utilized to fabricate support materials. Such materials are generally either synthetic or natural polymers, examples of useful synthetic polymers being polyethylene, polyacrylamide, nylon, resins, polyvinyl chloride, and polystyrene. Natural polymers typically used are cellulose, polysaccharides, Sepharose, agarose, and various dextrans. Additional material that can be employed to fabricate the support material are silica, particularly glass, collagen, and polynucleotides. While a variety of the materials described above will perform adequately in the subject invention, the preferred embodiment employs material composed of nylon.

An important aspect of the subject diagnostic device is the method of applying antibody to the solid matrix material

24. Most current methods non-selectively deposit antibody over the entire surface of the matrix material 24. This wastes antibody, which is often expensive or difficult to obtain, and, moreover, precludes assaying for more than one 5 antigen present in the same sample. We have found that both problems are eliminated by spray delivering antibody in a thin fluid stream on to the matrix material 24. This is best achieved by forcing a solution containing antibody through a small bore nozzle whereupon the solution is fragmented into 10 discrete droplets using sound vibrations or other means. The droplets are subsequently charged by passing through an electric field, and then deflected onto the matrix material 24. The procedures for effecting this method are described in U.S. patents 3,281,860 and 4,121,222, and are hereby 15 incorporated by reference.

The above process is most readily achieved using a commercial printing device manufactured by Videojet Systems International. The device is termed a Videojet Coder/Printer, and provides a stream of antibody under a 20 variety of conditions, and at varying stream widths. Using this device, it is possible to dispose a series of lines, or other patterns on the matrix material 24, each containing an antibody with different antigenic specificities.

It will be appreciated that spray application of 25 antibody to the matrix material 24 is suitable either when antibody is sought to be associated with the matrix material 24 by simple absorption, or by covalent attachment with chemically pretreated matrix material.

Figure 2 shows that situated beneath the solid matrix 30 material, is a mid-layer of material 22. The mid-layer is

situated between the absorbent material 20, and the matrix material 24, and acts to reduce the background of the assay. After the assay fluids pass through the matrix material 24, they contact, and filter through the mid-layer 22. The latter greatly reduces the background of the assay by reducing the backflow of unreacted reagents and thus keeps them from recontacting the matrix material 24. A wide variety of materials are suitable for forming the mid-layer 22. Particularly suitable is non woven polypropylene material commonly found in disposable diapers as described in U.S. Patents 3,860,003, 4,081,301, and 4,515,595.

In addition to the mid-layer 22, another feature of the present diagnostic device which results in low background, and enhances its simplicity of use, is the filtering device 28 associated with the top section 12. It comprises a funnel shaped central region 38 that readily accommodates an amount of assay fluid needed to perform the assay in a single application, and a tab 34 that permits the user to grasp and remove the device 28. At the bottom of the filter device 28 is filter material 36. This material is impregnated with one or more reagents needed to perform the assay, and which are carried down onto the matrix material 24 with assay fluid when the latter is applied to the filtering device 28.

25 A variety of materials can be used to fabricate the filtering material 36 in the filtering device 28. Indeed, for the most part those materials described supra that comprise the matrix material 24 can be suitably employed for the filtering material 36. We have found glass fiber is

particularly suitable, an example being Ultipor GF Filter U6-40, from Pall Corporation.

A variety of reagents can be impregnated into, dusted onto, or otherwise associated with the filter material 36.

- 5 It is particularly advantageous to have protein blocking agents associated with the filter material 36. The type of blocking agent is not critical. That is a variety of proteinaceous materials, amino acids, peptides can be suitably employed. However, we have found that milk protein
- 10 is satisfactory, and routinely use non-fat dry milk sold by Carnation Corporation. Additional, in those instances when the solid matrix material 24 is chemically pretreated to covalently bind antibody, it may be desirable to use small molecular weight amino reactive reagents such as glycine as
- 15 the blocking agent.

In order to effaciously associate blocking agent with the filter material 36, it is desirable to contact the filter material 36 with dry material for a time sufficient to uniformly coat the material. This can be accomplished by

- 20 contacting the filter material with the blocking agent, followed by removing any material that is not firmly adherent to the filter.

It will be appreciated that an alternative method of associating the blocking agent with the filter material 36 is to contact the material with a solution containing the blocking agent, and then lyophilize the material. This is particularly useful when small molecular weight (i.e. glycine) blocking agents are used. While filter material so treated will perform adequately in the present device, it is

- 25 not a preferred method because lyophilization causes the

filter to harden which in turn increases the time it takes for solutions to pass through the filter material. This results in uneven deposition of the blocking agent on the matrix material 24, and an increase in background.

5 In addition to having blocking agents associated with
the filter material 36 of the filtering device 28, it may
also be desirable to impregnate other reagents into the
material that are utilized in the assay, thereby avoiding
having to add these reagents in separate steps. For
10 example, it is anticipated that reagents used to reveal the
presence of the antibody-antigen complex, that is antibody
enzyme conjugates, or enzyme substrates, can be similarly
associated with the filter material 36.

A second feature of the subject invention alluded to above, that is important in establishing the long term room temperature stability of the diagnostic device, is the utilization of a suitable chemical drying agent situated in chamber 18 in the bottom section 14. The stability, or useful lifetime, of the materials in the matrix material 24, or the filter material 36, is a function of the humidity encountered by the device. Presently used immunodiagnostic devices have a useful shelf time of less than 6 months at room temperature, whereas the present device has a room temperature shelf time of up to one year. We have found that by associating a drying agent with the diagnostic device that the reagents remain stable and give outstanding performance over this time. A variety of drying agents are well known in the art, and are anticipated to be useful.

In order to detect the presence of the immune complex
30 on the matrix material 24, it is generally required that a

labeled second detector molecule be used. In those instance where the complex is an immune complex, the detector molecule is a second antibody having specificity for antigen bound to the first antibody, but binds to antigen at a site 5 remote from that where the first antibody is bound. Traditional methods of detecting the presence of antigen have utilized a labeled second antibody wherein the label is often a radioactive tracer, or more recently, an enzyme capable of hydrolyzing a colorless substrate to produce a 10 detectable color change, thereby revealing the immune complex. A variety of enzymes are usable in combination with the appropriate substrate. For example horseradish peroxidase, beta-galactosidase, glucose oxidase, alkaline phosphatase, and others well known to those skilled in the 15 art can be suitably employed. Most of these enzymes utilize diazonium or tetrazolium salts as substrates. Examples of the former are napthol AS MX phosphate and diazo 2-amino 5-chloro Anisol used as substrate for alkaline phosphatase.

Methods for associating enzymes with second antibody 20 are well known to those skilled in the art, and primarily involve chemically coupling the enzyme to the antibody. Procedures for coupling antibody by chemical cross-linking are described by O'Sullivan and Marks in *Methods in Enzymology*, (1981) (73:147) Academic Press, New York. If 25 horseradish peroxidase is used then a suitable coupling method is that of Nakane and Kanaoi described in the *Journal of Histology and Cytochemistry* (1974) (82:1084). This method effectively and directly conjugates the enzyme to the antibody; however other methods are well known, for example,

an biotin-avidin bridge can be formed on the second antibody having horseradish peroxidase linked to avidin.

In lieu of chemically coupling the enzyme to the second antibody-enzyme conjugate, it may be preferred to have the enzyme integrated into the antibody. This can be accomplished, for example by genetically engineering hybrid molecules having both an antibody binding site, and an enzyme active site. For instance, antibody can be modified by DNA recombinant techniques as described by Neuberger et al in Recombinant Antibody Possessing Novel Effector Function, Nature (1984) (312:604). It is anticipated that this type of enzyme conjugate can be directly incorporated into the filtering material 36 of the filtering device 28, or can be added in a subsequent step to reveal the immune complex formed on the matrix material 24.

It will be appreciated by those skilled in the art that the antibodies that are deposited on the matrix material 24, or that comprise the antibody-enzyme conjugate, can be either monoclonal or polyclonal. After the antibody-enzyme conjugate has been added to the matrix material 24 and sufficient time has passed to maximize binding of the antibody-enzyme conjugate to bound antigen, a solution containing a suitable enzyme substrate is added, and the appearance of color is noted as being indicative of the presence of the antigen in the assay sample. In most instances, it will not be necessary to insert a wash step after the conjugate has been added, and before the addition of substrate. This is because the funnel shape of the aperture 26 enables a large amount of substrate solution to pass through a small amount of surface area of the substrate

material. Thus, addition of the substrate solution in effect acts as a washing step. Nevertheless, however, for some applications it may be desirable to have a washing step to eliminate undesirable background.

5 The present invention will now be illustrated by the following examples. It will be apparent to those skilled in the art that there are a variety of substitutions possible for the material and methods employed. Consequently, the examples presented should be viewed as exemplary, and not as
10 limiting the invention to the particular materials or methods described.

Example 1

Detection of Chorionic Gonadotropin hormone (hCG)

This example will be described with reference to
15 Figures 1 and 2. An amount of urine corresponding to approximately 0.5 milliliters, and containing 25 mIU/ml hCG was applied to the filtering device 28. The urine contacts the filter material 36 of the filtering device 28, and passes through the filter material, carrying with it a
20 protein blocking agent, milk protein, impregnated in the filter material 36. The filtrate containing the blocking agent passes through the aperture 26, present in the top 12 and contacts the matrix material 24. The matrix material 24 is impregnated with antibodies to human hCG. The matrix
25 material was made of nylon, of a type well known and routinely used in the art.

Impregnation of the matrix material 24 was realized using a printer/coder machine as described in U.S. Patents 3,281,860 and 4,121,222 by applying a narrow stream of fluid
30 to the matrix material 24 containing mouse monoclonal

antibody directed against the alpha chain of hCG. The antibody was applied in approximately 1.5 millimeter wide lines. For convenience to the ultimate user of the device, antibody was applied in a vertical line, that passed across 5 a horizontal line of previously applied goat anti-mouse antibody of the IgG class. The latter will be explained in more detail infra. Application of antibody consists of spraying a solution containing 4 milligrams per milliliter of mouse monoclonal antibody against alpha chain of hCG in a 10 suitable buffer, phosphate buffer saline is satisfactory. This consists of 10 mM sodium phosphate with 150 mM sodium chloride, pH 7.1. In addition, the solution contained 100 micro-grams per milliliter of flourescein, and a bacteriostatic agent, such as, 0.1% sodium azide. 15 Flourescein is applied to the solution to provide a visual means for assessing the pattern of antibody formed on the matrix material 24.

After the filtrate has passed through the filter material 36, it contacts the matrix material 24. hCG 20 present in the filtrate binds to hCG antibody impregnated in the matrix material 24. In addition, simultaneously with this event, the blocking agent present in the filter 36 binds to the matrix material 24 at sites other than those to which the monoclonal antibody is bound. In so doing, these 25 sites are made unavailable for reaction with subsequently added reactants. A short time after the filtrate contacts the matrix material 24, two drops of a solution containing a second mouse monoclonal antibody enzyme conjugate is added. The second antibody is directed against beta 30 subunit of hCG, and binds to a different epitope than that

to which the first antibody that is attached to the matrix material is bound. The enzyme component of the conjugate was alkaline phosphatase. The antibody-enzyme conjugate passes through the filter material 36, and contacts the matrix material 24 for a time sufficient for the conjugate to react and combine with hCG bound to the first antibody. Generally this takes about 1 minute.

In order to reveal the complex formed on the matrix material 24, a solution containing substrate for alkaline phosphatase, indoxyl phosphate, was added directly to the matrix material 24. In about 1 minute, a blue color formed on the matrix material 24, in a "+" pattern indicating that the assay sample contains hCG. Should a "--" sign appear, the sample contains insignificant amounts of hCG. It is satisfactory if approximately 0.5 milliliters of the substrate solution containing 4 mM indoxyl phosphate is utilized.

Lastly, an amount of a suitable reaction stopping solution is added to the matrix material 24. 0.5 mls. of a solution containing 0.1% acetic acid performs satisfactorily.

The "+" pattern, as alluded to above, is realized by disposing anti-hCG first antibody in a vertical line over a horizontal line of either second antibody enzyme conjugate, enzyme alone, or goat anti-mouse antibody. The latter is preferred because it matches the type of reagent (i.e. protein antibody) used to form the vertical line of the "+" sign. Thus, any loss in activity over time in one reagent is balanced by a corresponding loss in the other. Regardless of which type of reagent is used to form the horizontal line,

they can be applied by being sprayed onto the matrix material 24 as described above.

Example 2

Room Temperature Stability

5 The materials and methods used in Example 1 can be similarly employed here. After storing a diagnostic device for one year at room temperature, it was successfully used to assay a sample containing 25mIU/ml of hCG.

Example 3

10 **Antigen Impregnation of the Matrix Material**

15 It will be apparent to those skilled in the art that the present diagnostic device is not limited to detecting antigens. It is equally possible to detect circulating antibodies present in the bodily fluids of a patient that has experienced a challenge to his immune system. This is done by attaching to the matrix material the antigen that is responsible for eliciting the immune response, and then assaying for the presence of antibody. This aspect of the diagnostic device is applicable, for example, in detecting, 20 or monitoring auto-immune, or allergy sufferers.

25 To demonstrate this aspect of the invention inactivated rubella virus can be attached to the matrix material 24 shown in Figure 2, using a printer coder machine described in Example 1. Subsequently, a solution containing anti-virus antibody to be detected is added to the filtering device 28 shown in Figure 2, and flows through the filter material 36, thereby producing a filtrate that passes through the aperture 26. The filtrate contacts the matrix material 24 containing bound virus. Anti-rubella virus antibody binds to 30 the virus on the matrix, and the detection of anti-rubella

antibody in the filtrate is then achieved by passing a solution containing antibody enzyme-conjugate, wherein the antibody is directed against bound anti-rubella antibody. The antibody component of the conjugate need only be capable
5 of recognizing an epitope on the anti-rubella antibody to be effective. Assuming that the anti-rubella antibody being assayed is human, then the antibody component of the conjugate should be antihuman antibody. The remaining steps in this assay are analogous to those described in Example 1.
10 The end result is the appearance of color on the matrix material 24 indicative of the presence of anti-rubella antibody in the assay fluid.

Example 4

Impregnation of the Filter Material with Assay Reagents
15 One of the goals in diagnostic testing is to develop a test device that requires few manipulative steps. By associating assay reagents with the filter material 36 of the filter device 28, it is possible to eliminate those steps whereby the reagents are added separately to the
20 matrix material 24 to carry out the assay.

Impregnation of the filter material 36 with proteinaceous blocking agents was achieved by pulverizing milk powder obtained from non-fat dry milk (Carnation Corporation), and sifted to remove any large granules still
25 present. Next, the filter material made of glass fibers (pre-filter grade Ultipor GF Filter U6-40, Pall Corporation) was cut into two by two centimeter squares, and were stored in a closed container with a suitable drying agent. The papers were then mixed with pulverized milk powder for a
30 time sufficient to impregnate the filters with milk powder,

generally this requires approximately three hours. Uniform association of the milk powder with the filter was accomplished by tumbling, or otherwise agitating the filters while in contact with the powder.

5 Excess milk powder was removed from the filter squares by sifting through a flour sieve, and then the filter was transferred to a container where they were shaken for a time sufficient to remove any loose milk powder present. Generally, this requires about one hour. This step was
10 followed by a second sifting step to remove any excess milk powder that was not earlier removed. The filters were stored in a container in the presence of a suitable drying agent. Filters prepared by this technique are directly usable in the diagnostic test device.

15

Example 5

Detection of Multiple Antigens

The materials and methods described in this Example are similar to those of Example 1 with the following exceptions. The matrix material 24 is treated with 2 antibodies having distinct antigenic specificities, one directed against the beta subunit of luteinizing hormone (LH) and the other against the beta subunit of follicle stimulating hormone (FSH). Using a printer coder machine described in Example 1, the antibodies can be deposited in discrete patterns on the matrix material 24. The second antibody that comprises the antibody enzyme-conjugate for detection of either LH or FSH can be either a single monoclonal antibody that recognizes a common epitope on LH and FSH, or two monoclonal antibodies that bind to different epitopes on LH and FSH.
30 In the latter case, two different enzymes that yield

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distinct color reactions can be bound to the monoclonal antibodies to produce distinct colored "+" signs. For example, alkaline phosphatase, and B-galactosidase can be used, the former gives a red color with a proper substrate, 5 and the latter a blue color.

Lastly, the horizontal line component of the "+" sign for LH and FSH can be formed as described in Example I.

Example 6

Sensitivity of the Diagnostic Device

10 The materials and methods described in Example 1 are employed here to compare the sensitivity and time of performance of the present device with presently used commercial devices. For each of the commercial devices the manufacturers procedures were followed. Solutions 15 containing varying amounts of hCG were tested and table 2 shows the detectable lower limit, or sensitivity of the devices. Also shown in the table is the method on which the assay is premised, types of antibodies, and the time it takes to perform the assay.

20 The invention described above has been described with respect to the use of specific materials and methods. However, it will be apparent to those skilled in the art that the invention is not so limited. Indeed, it is readily apparent that there exists numerous equivalent materials and 25 methods that may be resorted to without departing from the spirit and scope of the invention.

We claim: